

## Graham's plasma time-activity curve model for parent tracer and a metabolite

This document describes the Graham's input function model [Graham, 1997], extended with compartments for a single labelled plasma metabolite, and the mathematical equations required for simulating them. The ODEs are solved using the second-order Adams-Moulton method with trapezoidal rule [Kuwabara et al., 1993].

### Model description

#### Compartmental model

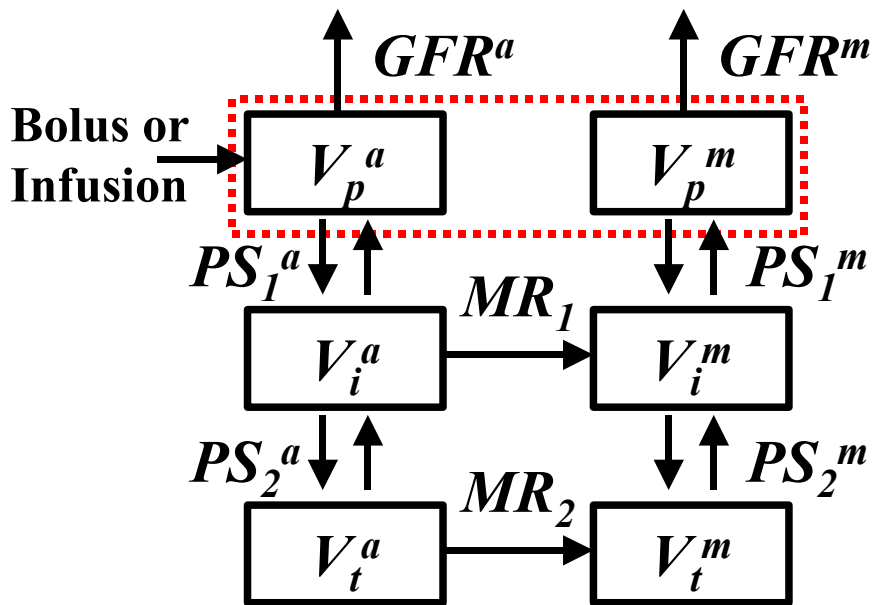


Fig. B1-1. Grahams's compartmental model extended with compartments for a metabolite.

**Table B1-1.** Descriptions of the model parameters.

|          |   |                          |
|----------|---|--------------------------|
| $C_p^a$  | Concentration of parent tracer in plasma  | $kBq\ mL^{-1}$           |
| $C_i^a$  | Concentration of parent tracer in interstitial fluid                            | $kBq\ mL^{-1}$           |
| $C_t^a$  | Concentration of parent tracer in tissue fluid                                  | $kBq\ mL^{-1}$           |
| $V_p^a$  | Volume of plasma for parent tracer  | $mL\ mL^{-1}$            |
| $V_i^a$  | Volume of interstitial fluid for parent tracer                                  | $mL\ mL^{-1}$            |
| $V_t^a$  | Volume of tissue fluid for parent tracer  | $mL\ mL^{-1}$            |
| $PS_1^a$ | Permeability-surface area product ( $PS$ ) for exchange from $V_p^a$ to $V_i^a$ | $mL\ min^{-1}\ mL^{-1}$  |
| $PS_2^a$ | $PS$ for exchange from $V_i^a$ to $V_t^a$                                       | $mL\ min^{-1}\ mL^{-1}$  |
| $GFR^a$  | Glomerular filtration rate for parent tracer                                    | $mL\ min^{-1}\ mL^{-1}$  |
| $MR_1$   | Rate of metabolism in interstitial volume                                       | $mL\ min^{-1}\ mL^{-1}$  |
| $MR_2$   | Rate of metabolism in tissue fluid volume                                       | $mL\ min^{-1}\ mL^{-1}$  |
| $C_p^m$  | Concentration of metabolized tracer in plasma                                   | $kBq\ mL^{-1}$           |
| $C_i^m$  | Concentration of metabolized tracer in interstitial fluid                       | $kBq\ mL^{-1}$           |
| $C_t^m$  | Concentration of metabolized tracer in tissue fluid                             | $kBq\ mL^{-1}$           |
| $V_p^m$  | Volume of plasma for metabolized tracer   | $mL\ mL^{-1}$            |
| $V_i^m$  | Volume of interstitial fluid for metabolized tracer                             | $mL\ mL^{-1}$            |
| $V_t^m$  | Volume of tissue fluid for metabolized tracer                                   | $mL\ mL^{-1}$            |
| $PS_1^m$ | $PS$ for exchange from $V_p^m$ to $V_i^m$                                       | $mL\ min^{-1}\ mL^{-1}$  |
| $PS_2^m$ | $PS$ for exchange from $V_i^m$ to $V_t^m$                                       | $mL\ min^{-1}\ mL^{-1}$  |
| $GFR^m$  | Glomerular filtration rate for metabolized tracer                               | $mL\ min^{-1}\ mL^{-1}$  |
| $H$      | Amount of activity infused per min  | $kBq\ min^{-1}\ mL^{-1}$ |
| $H'$     | $H$ at the end of the infusion period;<br>$H'=H*(1-exp(-k*Dur))$                | $kBq\ min^{-1}\ mL^{-1}$ |
| $k$      | Time constant   | $min^{-1}$               |
| $Delay$  | Time before bolus reaches the measurement point                                 | $min$                    |
| $Dur$    | Duration of infusion; in bolus injection $Dur=0$                                | $min$                    |

## Simulation of bolus and infusion

The equations for bolus input (1) and infusion (2) are:

$$Input(t) = \begin{cases} 0 & , t < Delay \\ H \times e^{-k(t-Delay)} & , t \geq Delay \end{cases} \quad (1)$$

$$Input(t) = \begin{cases} 0 & , t < Delay \\ H \times (1 - e^{-k(t-Delay)}) & , Delay \leq t < Delay + Dur \\ H \times e^{-k(t-Delay-Dur)} & , t \geq Delay + Dur \end{cases} \quad (2)$$

## Integral of input

The equations for bolus injection integral from time 0 to T is

$$\int_0^T Input(t) dt = \begin{cases} 0 & , T < Delay \\ \frac{H}{k} (1 - e^{-k(T-Delay)}) & , T \geq Delay \end{cases} \quad (3)$$

and for infusion integral:

$$\int_0^T Input(t) dt = \begin{cases} 0 & , T < Delay \\ H(T - Delay) - \frac{H}{k} (1 - e^{-k(T-Delay)}) & , Delay \leq T < Delay + Dur \\ H \times Dur - \frac{H}{k} (1 - e^{-k \times Dur}) e^{-k \times (T-Delay-Dur)} & , T \geq Delay + Dur \end{cases} \quad (4)$$

## Differential equations for the concentrations in model compartments

$$V_p^a \frac{dC_p^a(t)}{dt} = Input(t) - (PS_1^a + GFR^a) \times C_p^a(t) + PS_1^a \times C_i^a(t) \quad (5)$$

$$V_i^a \frac{dC_i^a(t)}{dt} = PS_1^a \times C_p^a(t) + PS_2^a \times C_i^a(t) - (PS_1^a + PS_2^a + MR_1) \times C_i^a(t) \quad (6)$$

$$V_i^a \frac{dC_i^a(t)}{dt} = PS_2^a \times C_i^a(t) - (PS_2^a + MR_2) \times C_i^a(t) \quad (7)$$

$$V_p^m \frac{dC_p^m(t)}{dt} = PS_1^m \times C_i^m(t) - (PS_1^m + GFR^m) \times C_p^m(t) \quad (8)$$

$$V_i^m \frac{dC_i^m(t)}{dt} = MR_1 \times C_i^a(t) + PS_1^m \times C_p^m(t) + PS_2^m \times C_i^m(t) - (PS_1^m + PS_2^m) \times C_i^m(t) \quad (9)$$

$$V_i^m \frac{dC_i^m(t)}{dt} = MR_2 \times C_i^a(t) + PS_2^m \times C_i^m(t) - PS_2^m \times C_i^m(t) \quad (10)$$

## Solving differential equations

Integration of Eq. (7) and solving using the second order Adams-Moulton method with trapezoidal rule (concentrations at time 0 are assumed to be 0) gives the equations for the concentration of parent tracer in tissue compartment and its integral:

$$C_i^a(T) = \frac{PS_2^a \int_0^T C_i^a(t) dt - (PS_2^a + MR_2) \left[ \int_0^{T-\Delta t} C_i^a(t) dt + \frac{\Delta t}{2} C_i^a(T - \Delta t) \right]}{V_i^a + \frac{\Delta t}{2} (PS_2^a + MR_2)} \quad (11)$$

$$\int_0^T C_i^a(t) dt = \frac{PS_2^a \frac{\Delta t}{2} \int_0^T C_i^a(t) dt + V_i^a \left[ \int_0^{T-\Delta t} C_i^a(t) dt + \frac{\Delta t}{2} C_i^a(T - \Delta t) \right]}{V_i^a + \frac{\Delta t}{2} (PS_2^a + MR_2)} \quad (12)$$

Integration of Eq. (6), substitution of Eq. (12) and solving gives the equations for the concentration of parent tracer in interstitial volume and its integral:

$$C_i^a(T) = \frac{\left\{ \begin{array}{l} PS_1^a \int_0^T C_p^a(t) dt + AV_i^a \left[ \int_0^{T-\Delta t} C_i^a(t) dt + \frac{\Delta t}{2} C_i^a(T - \Delta t) \right] \\ - (PS_1^a + MR_1 + PS_2^a (1 - \frac{\Delta t}{2} A)) \left[ \int_0^{T-\Delta t} C_i^a(t) dt + \frac{\Delta t}{2} C_i^a(T - \Delta t) \right] \end{array} \right\}}{V_i^a + \frac{\Delta t}{2} (PS_1^a + MR_1 + PS_2^a (1 - \frac{\Delta t}{2} A))} \quad (13)$$

$$\int_0^T C_i^a(t) dt = \frac{\left\{ \begin{array}{l} PS_1^a \frac{\Delta t}{2} \int_0^T C_p^a(t) dt + AV_i^a \frac{\Delta t}{2} \left[ \int_0^{T-\Delta t} C_i^a(t) dt + \frac{\Delta t}{2} C_i^a(T - \Delta t) \right] \\ + V_i^a \left[ \int_0^{T-\Delta t} C_i^a(t) dt + \frac{\Delta t}{2} C_i^a(T - \Delta t) \right] \end{array} \right\}}{V_i^a + \frac{\Delta t}{2} (PS_1^a + MR_1 + PS_2^a (1 - \frac{\Delta t}{2} A))} \quad (14)$$

, where  $A = PS_2^a / (V_i^a + (\Delta t/2) * (PS_2^a + MR_2))$ . Integration of Eq. (5), substitution of Eq. (14) and solving gives the equation for the concentration of parent tracer in plasma volume:

$$C_p^a(T) = \frac{\left\{ \begin{array}{l} \int_0^T Input(t) dt \\ - (GFR^a + PS_1^a (1 - \frac{\Delta t}{2} B)) \left[ \int_0^{T-\Delta t} C_p^a(t) dt + \frac{\Delta t}{2} C_p^a(T - \Delta t) \right] \\ + A B V_i^a \frac{\Delta t}{2} \left[ \int_0^{T-\Delta t} C_i^a(t) dt + \frac{\Delta t}{2} C_i^a(T - \Delta t) \right] \\ + B V_i^a \left[ \int_0^{T-\Delta t} C_i^a(t) dt + \frac{\Delta t}{2} C_i^a(T - \Delta t) \right] \end{array} \right\}}{V_p^a + \frac{\Delta t}{2} (GFR^a + PS_1^a (1 - \frac{\Delta t}{2} B))} \quad (15)$$

, where  $B = PS_1^a / (V_i^a + (\Delta t/2) * (PS_1^a + MR_1 + PS_2^a * (1 - (\Delta t/2) * A)))$ .

Integration of Eq. (10) and solving gives equations for the concentration of labeled metabolite in tissue volume and its integral:

$$C_t^m(T) = \frac{MR_2 \int_0^T C_t^a(t) dt + PS_2^m \int_0^T C_i^m(t) dt - PS_2^m \left[ \int_0^{T-\Delta t} C_t^m(t) dt + \frac{\Delta t}{2} C_t^m(T - \Delta t) \right]}{V_t^m + \frac{\Delta t}{2} PS_2^m} \quad (16)$$

$$\int_0^T C_t^m(t) dt = \frac{MR_2 \frac{\Delta t}{2} \int_0^T C_t^a(t) dt + PS_2^m \frac{\Delta t}{2} \int_0^T C_i^m(t) dt + V_t^m \left[ \int_0^{T-\Delta t} C_t^m(t) dt + \frac{\Delta t}{2} C_t^m(T - \Delta t) \right]}{V_t^m + \frac{\Delta t}{2} PS_2^m} \quad (17)$$

Integration of Eq. (9), substitution of Eq. (17) and solving gives the equations for the concentration of metabolite in intersitial volume and its integral:

$$C_i^m(T) = \frac{\left\{ \begin{aligned} &MR_1 \int_0^T C_i^a(t) dt + PS_1^m \int_0^T C_p^m(t) dt + D MR_2 \frac{\Delta t}{2} \int_0^T C_i^a(t) dt \\ &+ D V_t^m \left[ \int_0^{T-\Delta t} C_t^m(t) dt + \frac{\Delta t}{2} C_t^m(T - \Delta t) \right] \\ &- \left( PS_1^m + PS_2^m \left( 1 - \frac{\Delta t}{2} D \right) \right) \left[ \int_0^{T-\Delta t} C_i^m(t) dt + \frac{\Delta t}{2} C_i^m(T - \Delta t) \right] \end{aligned} \right\}}{V_i^m + \frac{\Delta t}{2} (PS_1^m + PS_2^m (1 - \frac{\Delta t}{2} D))} \quad (18)$$

$$\int_0^T C_i^m(t) dt = \frac{\left\{ \begin{aligned} &MR_1 \frac{\Delta t}{2} \int_0^T C_i^a(t) dt + PS_1^m \frac{\Delta t}{2} \int_0^T C_p^m(t) dt + D MR_2 \left( \frac{\Delta t}{2} \right)^2 \int_0^T C_i^a(t) dt \\ &+ D V_t^m \frac{\Delta t}{2} \left[ \int_0^{T-\Delta t} C_t^m(t) dt + \frac{\Delta t}{2} C_t^m(T - \Delta t) \right] \\ &+ V_i^m \left[ \int_0^{T-\Delta t} C_i^m(t) dt + \frac{\Delta t}{2} C_i^m(T - \Delta t) \right] \end{aligned} \right\}}{V_i^m + \frac{\Delta t}{2} (PS_1^m + PS_2^m (1 - \frac{\Delta t}{2} D))} \quad (19)$$

, where  $D = PS_2^m / (V_t^m + (\Delta t/2) * PS_2^m)$ . Integration of Eq. (8), substitution of Eq. (19) and solving gives the equation for the concentration of metabolized tracer in plasma volume:

$$C_p^m(T) = \frac{\left\{ \begin{aligned} &E MR_1 \frac{\Delta t}{2} \int_0^T C_i^a(t) dt + D E MR_2 \left( \frac{\Delta t}{2} \right)^2 \int_0^T C_i^a(t) dt \\ &- \left( GFR^m + PS_1^m \left( 1 - \frac{\Delta t}{2} E \right) \right) \left[ \int_0^{T-\Delta t} C_p^m(t) dt + \frac{\Delta t}{2} C_p^m(T - \Delta t) \right] \\ &+ D E V_t^m \frac{\Delta t}{2} \left[ \int_0^{T-\Delta t} C_t^m(t) dt + \frac{\Delta t}{2} C_t^m(T - \Delta t) \right] \\ &+ E V_i^m \left[ \int_0^{T-\Delta t} C_i^m(t) dt + \frac{\Delta t}{2} C_i^m(T - \Delta t) \right] \end{aligned} \right\}}{V_p^m + \frac{\Delta t}{2} (GFR^m + PS_1^m (1 - \frac{\Delta t}{2} E))} \quad (20)$$

, where  $E = PS_1^m / (V_i^m + (\Delta t/2) * (PS_1^m + PS_2^m * (1 - (\Delta t/2) * D)))$ .

The original Graham's model can be derived from the extended model by setting the parameters of the extension compartment ( $PS_3, V_c$ ) to zero.

## References

1. Graham MM. Physiologic smoothing of blood time-activity curves for PET data analysis. *J. Nucl. Med.* 1997; 38: 1161-1168.
2. Kuwabara H, Cumming P, Reith J, Léger G, Diksic M, Evans AC, Gjedde A. Human striatal L-DOPA decarboxylase activity estimated in vivo using 6- $[^{18}\text{F}]$ fluoro-DOPA and positron emission tomography: error analysis and application to normal subjects. *J. Cereb. Blood Flow Metab.* 1993; 13:43-56.